

ISP Group

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22/01/2014

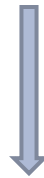
You know certainly about some of these situations...

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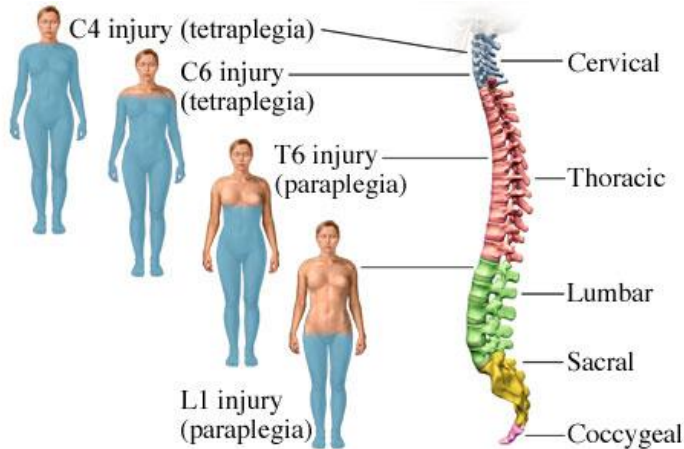


The falls are an important cause of spinal cord injuries

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For now, only subjective tests are used to evaluate the functional damage



Consequences depends on the lesion site but also on the extent of the damage

ASIA test based on the feelings of the patient

Patient Name _____
Examiner Name _____ Date/Time of Exam _____

ASIA STANDARD NEUROLOGICAL CLASSIFICATION OF SPINAL CORD INJURY **ISCS**

MOTOR
KEY MUSCLES (scoring on weaker side)

C5	R	Elbow flexors
C5	L	Elbow flexors
C6	R	Wrist extensors
C6	L	Wrist extensors
C7	R	Elbow extensors
C7	L	Elbow extensors
C8	R	Finger flexors (distal phalanx of little finger)
C8	L	Finger flexors (distal phalanx of little finger)
T1	R	Finger abductors (middle finger)
T1	L	Finger abductors (middle finger)

UPPER LIMB TOTAL (MAXIMUM) (25) (25) (50)

SENSORY
KEY SENSORY POINTS

0 = absent
1 = impaired
2 = normal
NT = not testable

Light Touch and Pin Prick scales for C2-C8, T1-T12, L1-L5, S1-S3.

Lower Limb Key Muscles:
L2: Hip flexors
L3: Knee extensors
L4: Ankle dorsiflexors
L5: Long toe extensors
S1: Ankle plantar flexors

Voluntary anal contraction (Yes/No)

Any anal sensation (Yes/No)

LOWER LIMB TOTAL (MAXIMUM) (20) (20) (40)

TOTALS (MAXIMUM) (90) (90) (180)

NEUROLOGICAL LEVEL: R L

COMPLETE OR INCOMPLETE? COMPLETE INCOMPLETE

ZONE OF PARTIAL PRESERVATION: NONE PARTIAL

ASIA IMPAIRMENT SCALE: A B C D E

Key Sensory Points: C2, C3, C4, C5, C6, C7, C8, T1, T2, T3, T4, T5, T6, T7, T8, T9, T10, T11, T12, L1, L2, L3, L4, L5, S1, S2, S3

Could we objectively quantify the functional loss after spinal cord injury?

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The technique should be able to...

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... evaluate the degeneration of the nervous fibers

... give an objective measure of the functional loss

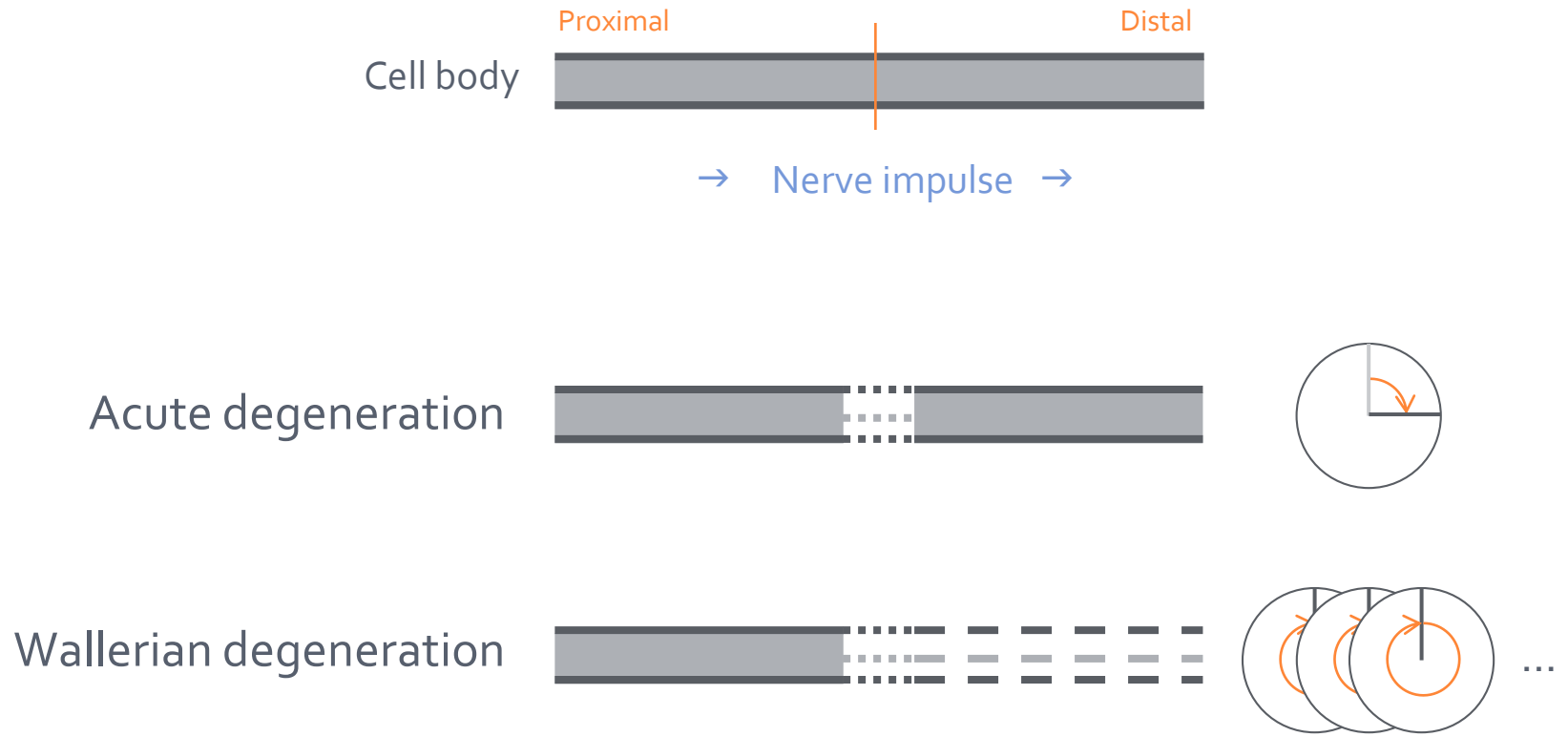
... provide longitudinal data of the patient

... consider the variability between subjects

In vivo evaluation of the **axonal degeneration**
after spinal cord injury
using diffusion MRI and DKI

The axonal degeneration is a two-step process

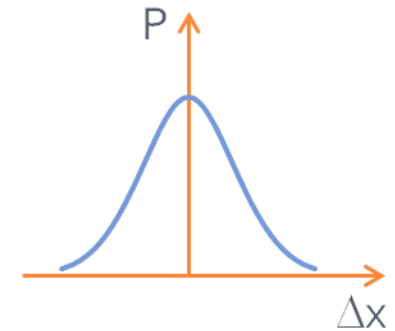
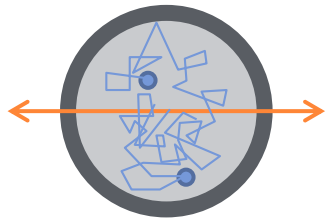
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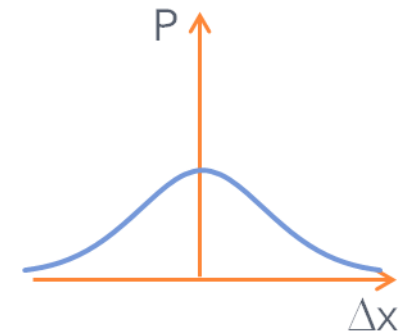
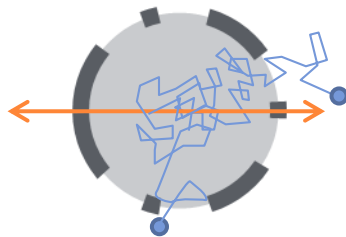
As a result, the diffusion of water molecules is altered

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Before damage



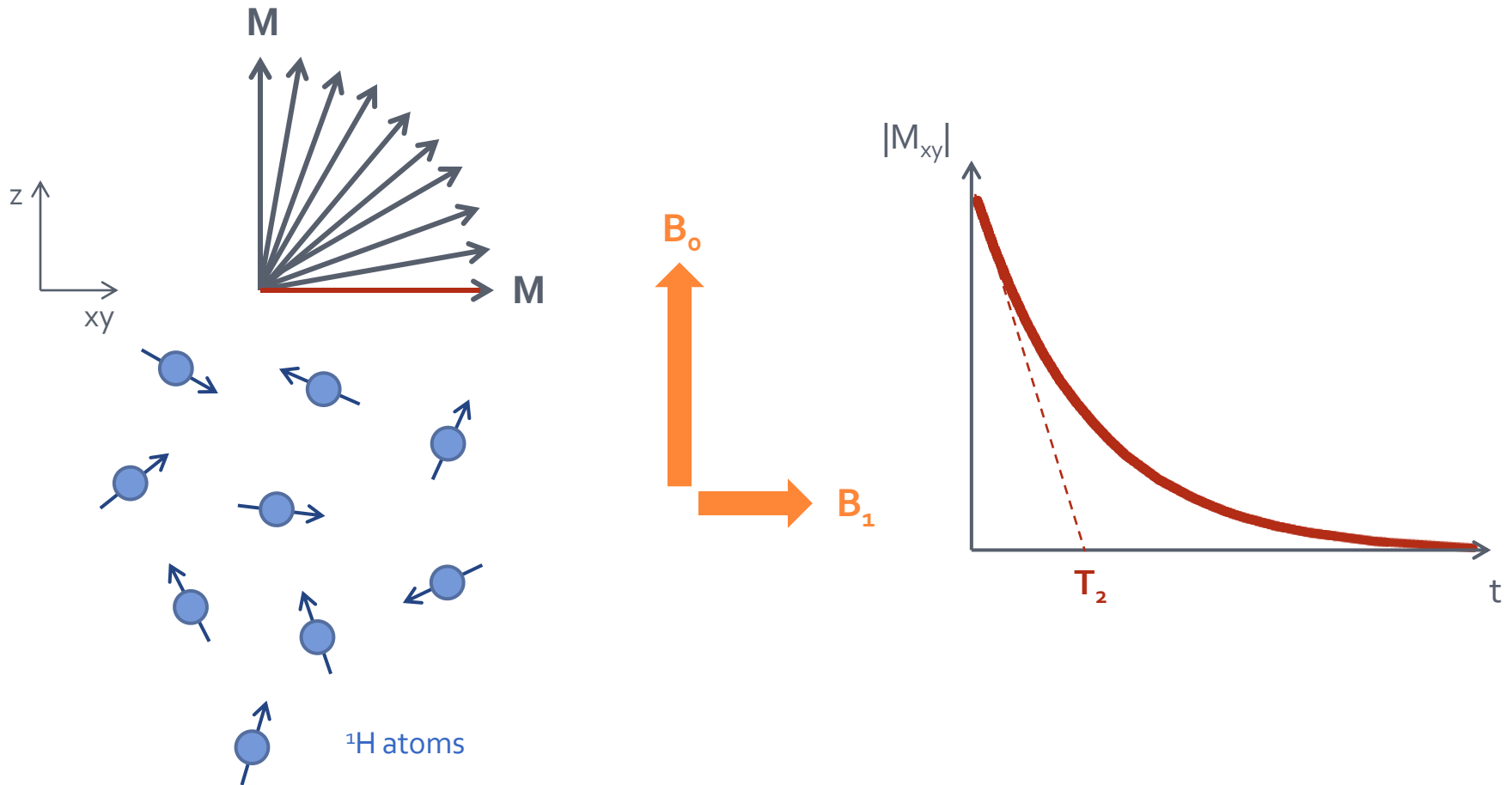
After damage



In vivo evaluation of the axonal degeneration
after spinal cord injury
using **diffusion MRI** and DKI

The MR signal measures the return to the equilibrium of the transverse magnetization after perturbation

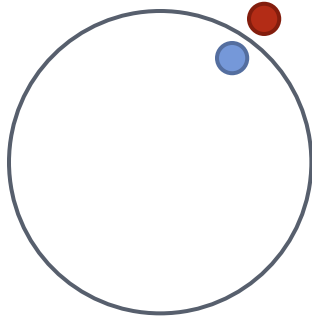
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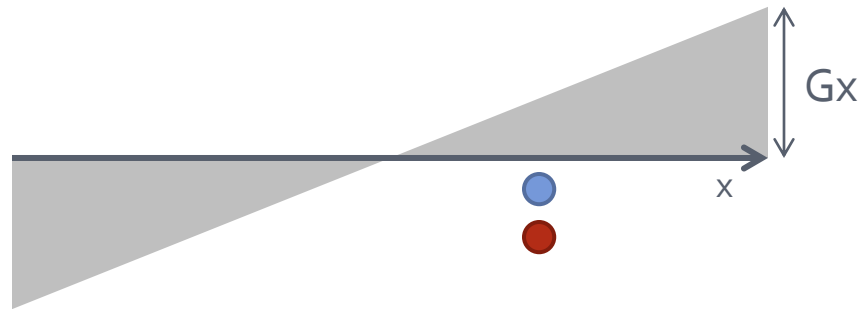
The more the molecules diffuse, the more the signal is attenuated

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Phase



Location

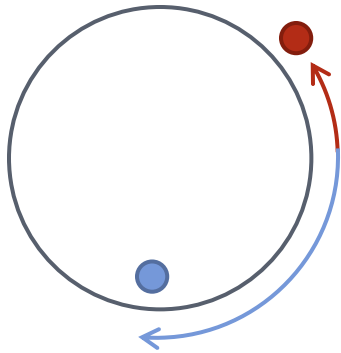


$$t = \delta$$

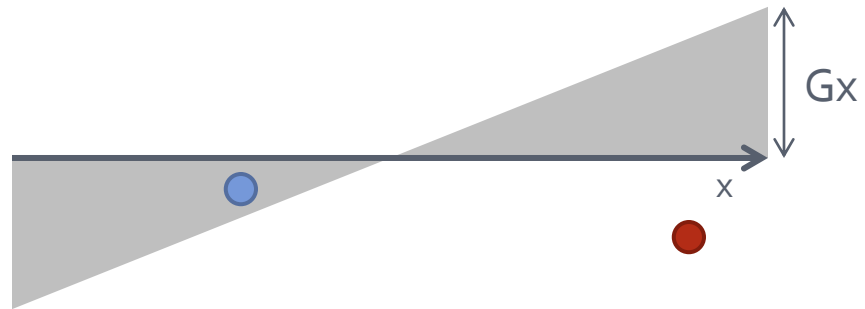
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Location

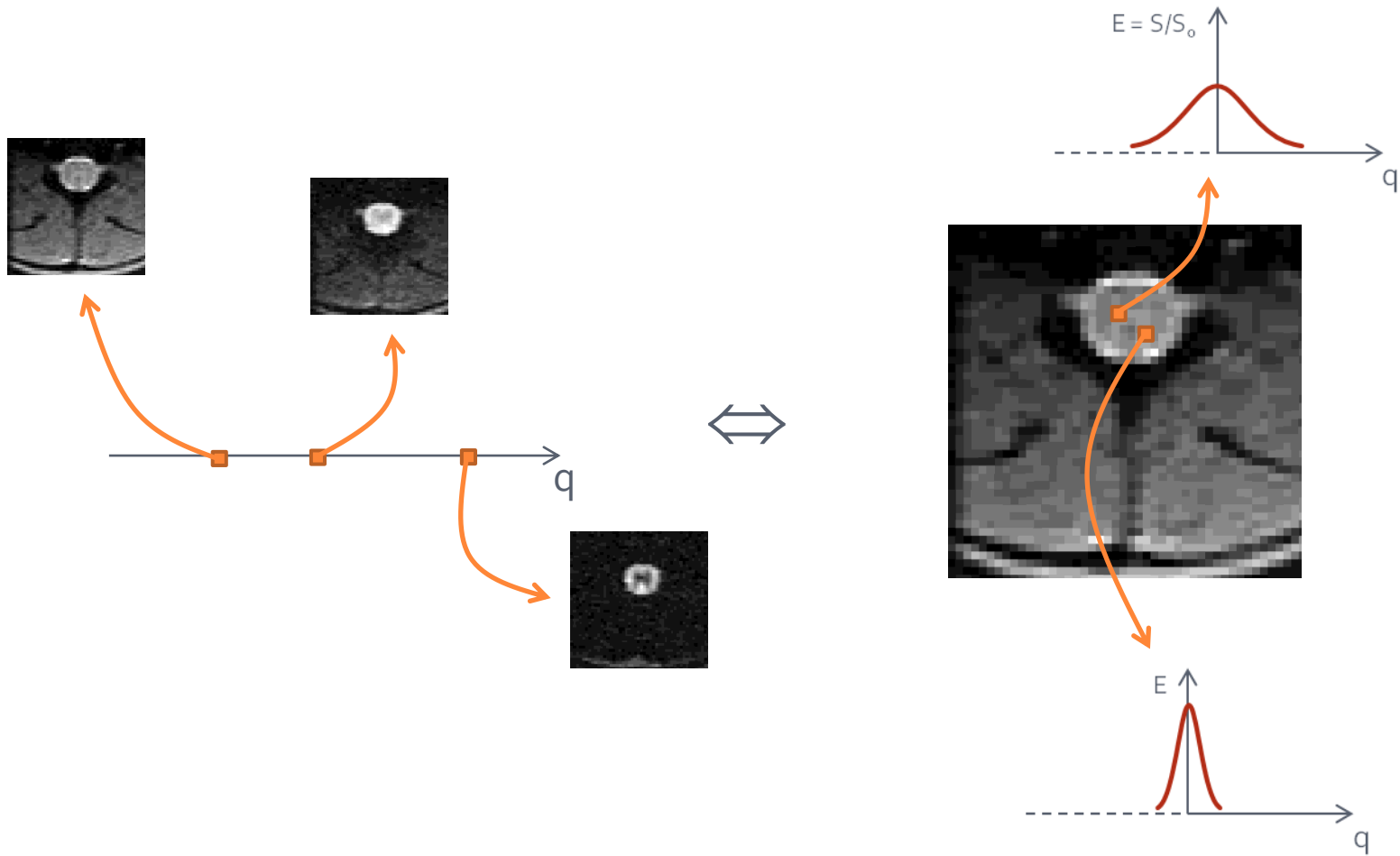


$$t = \Delta + \delta$$

$$\mathbf{q} = \gamma / 2\pi \delta \mathbf{G} \hat{\mathbf{I}}_x$$

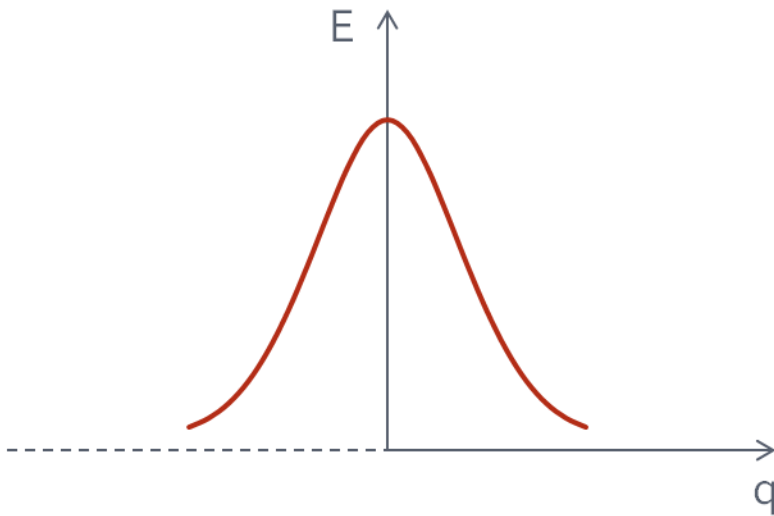
A diffusion weighted image is obtained for each q-value

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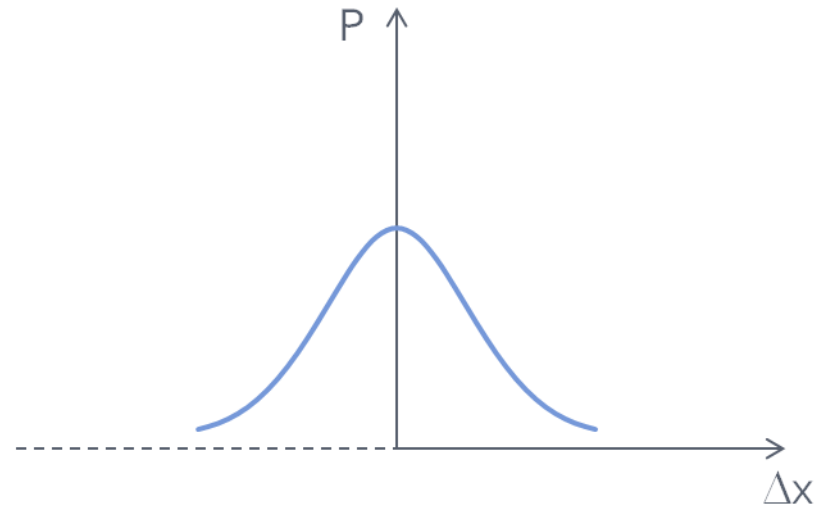


What is the relation between the signal attenuation and the probability density function of displacement?

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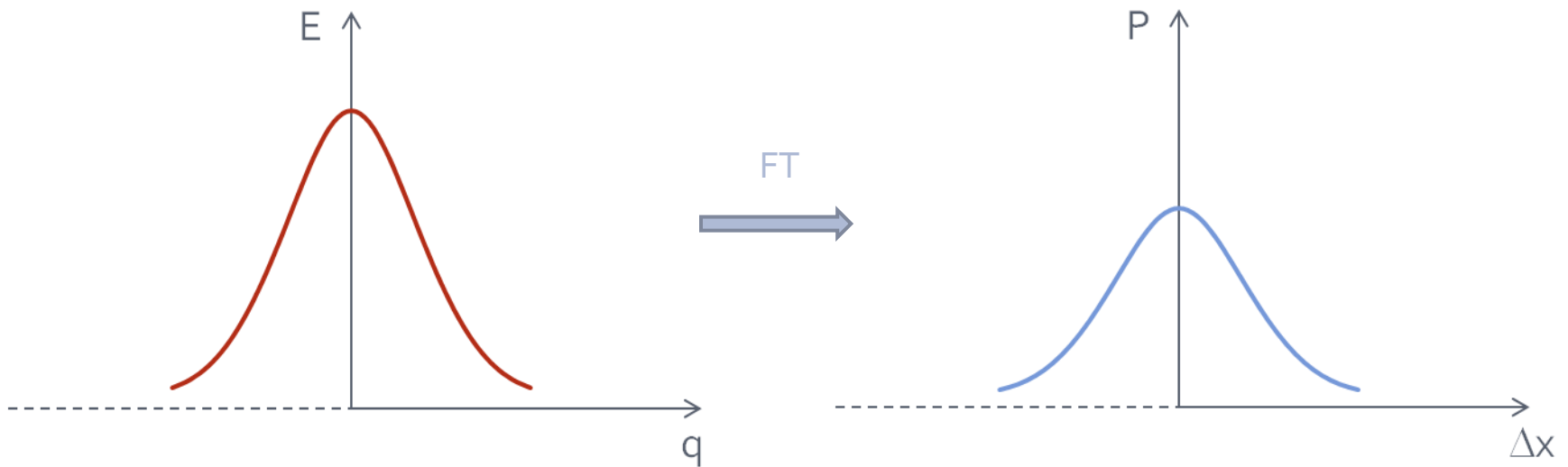


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The pdf is obtained applying a Fourier Transform to the signal attenuation curve

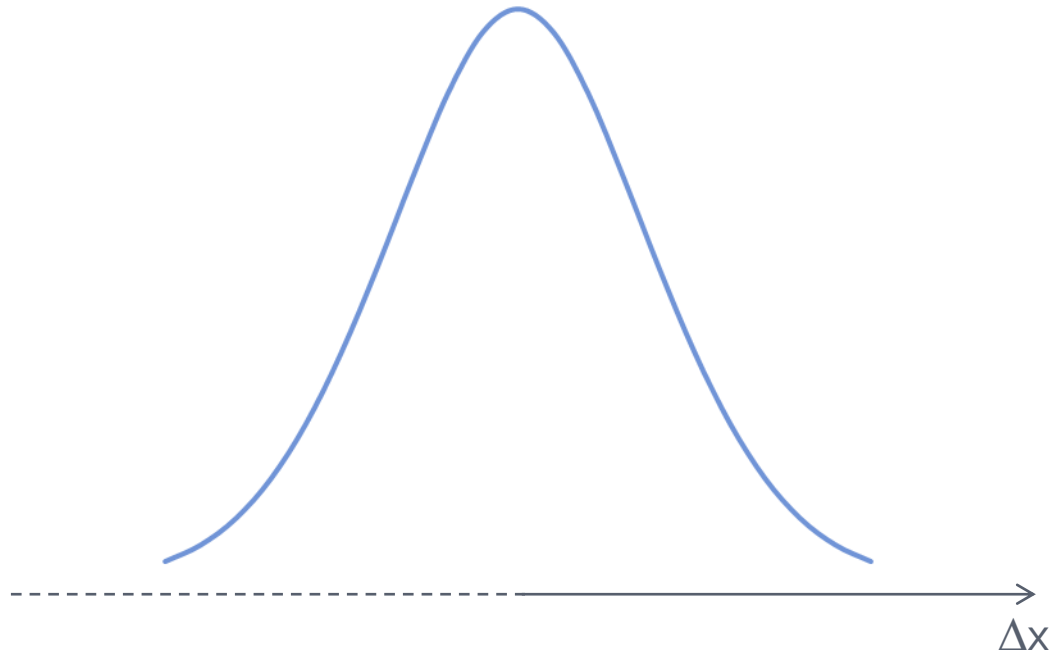
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$$P(\Delta x) = \int_q E(q) e^{-i2\pi q \Delta x} dq$$

The diffusion can be characterized by different properties

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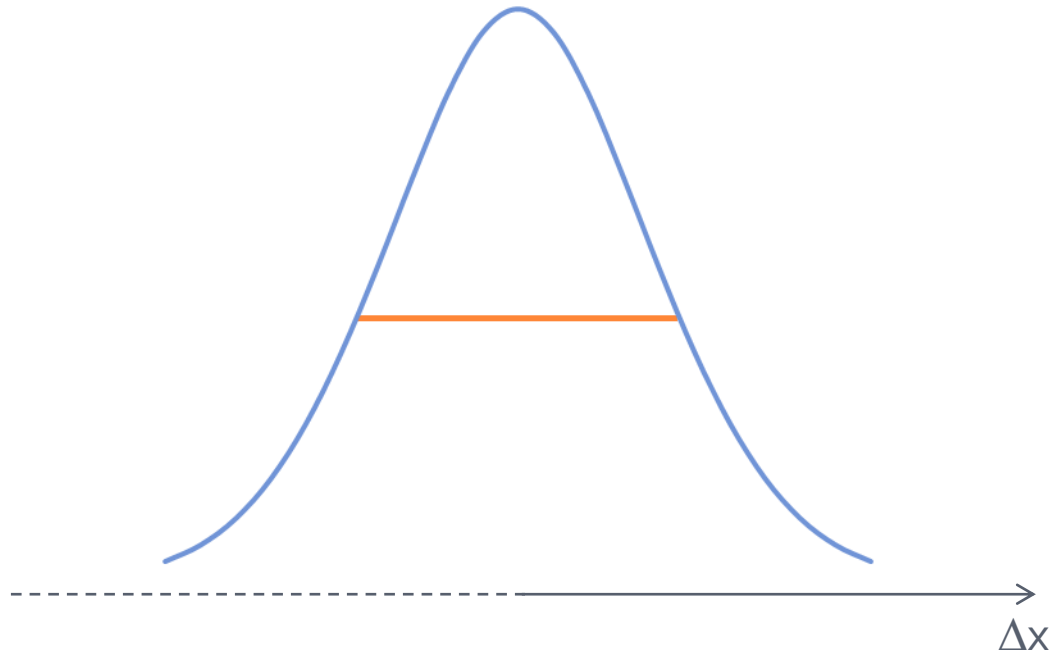
Full Width at Half Maximum (FWHM)

Return to Origin Probability (RTOP)

Kurtosis

The diffusion can be characterized by different properties

12



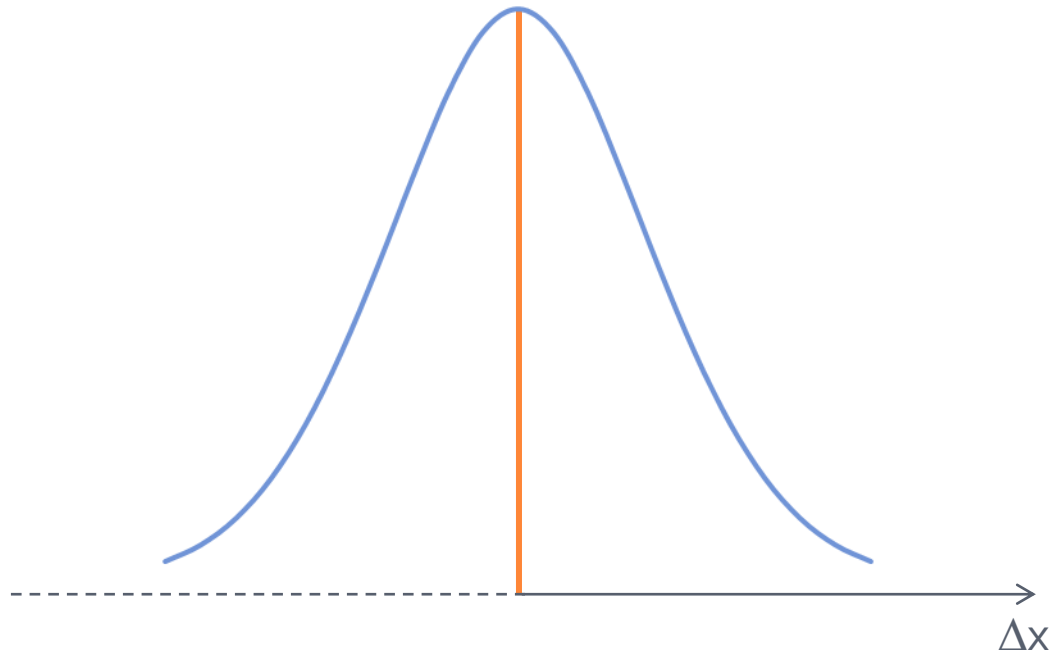
Full Width at Half Maximum (FWHM)

Return to Origin Probability (RTOP)

Kurtosis

The diffusion can be characterized by different properties

12



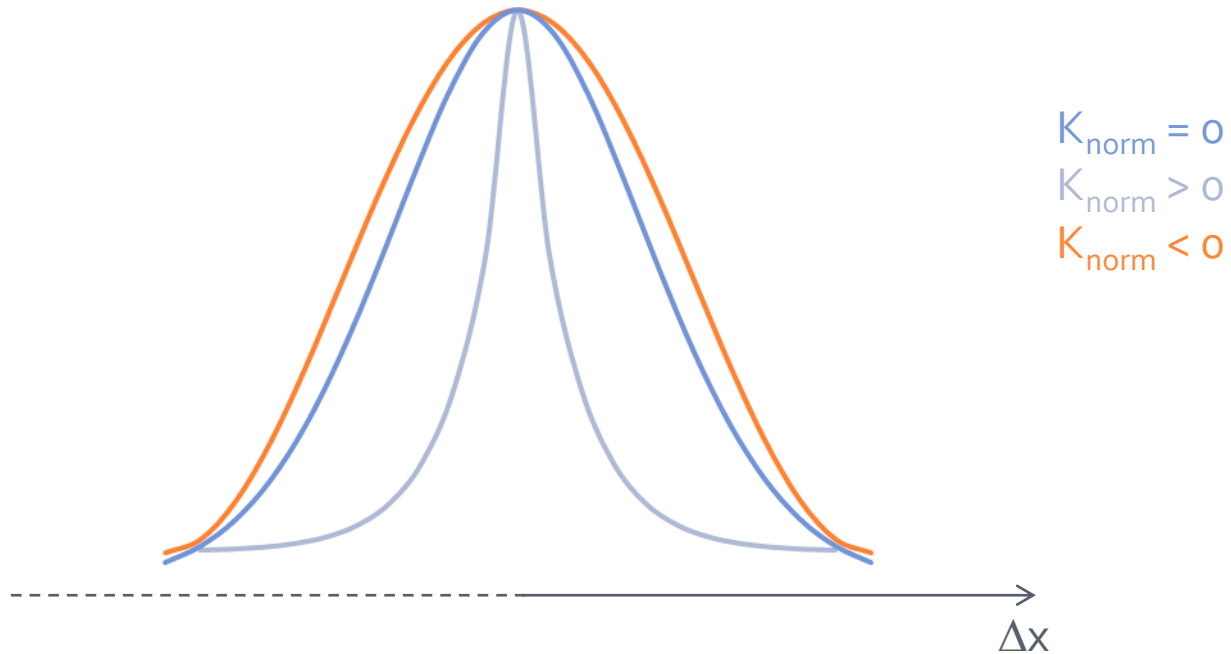
Full Width at Half Maximum (FWHM)

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The diffusion can be characterized by different properties

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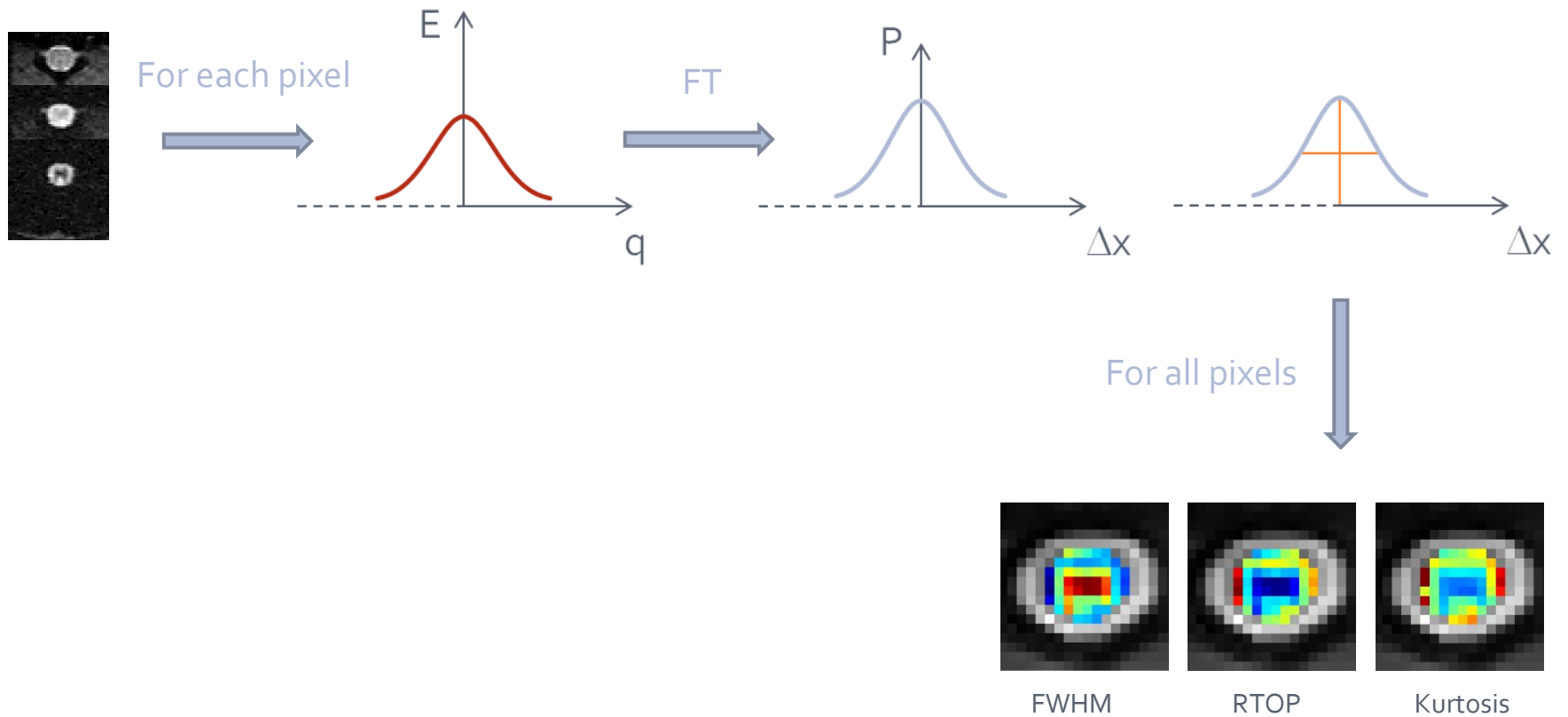
Full Width at Half Maximum (FWHM)

Return to Origin Probability (RTOP)

Kurtosis

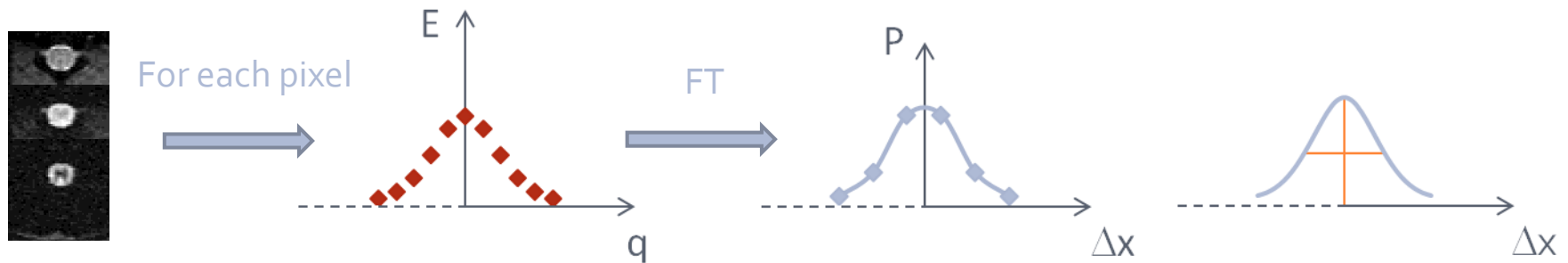
From acquisitions to diffusion maps: the ideal case

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In practice, the signal is measured only for several q-values

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In real conditions...

Observations corrupted by noise

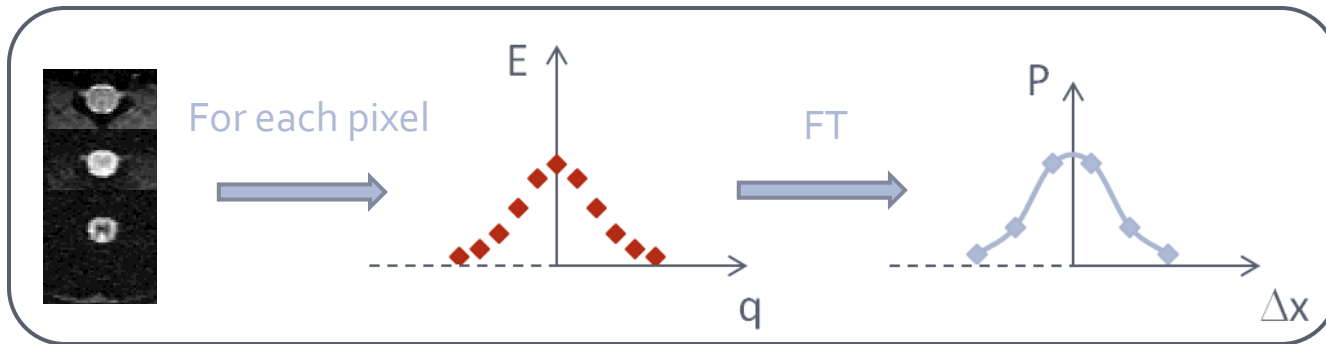
Finite number of observations and limited resolution in the spatial domain

Artifacts (movements, partial volume effect, etc.)

...

In practice, the signal is measured only for several q-values

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In real conditions...

Observations corrupted by noise

Finite number of observations and limited resolution in the spatial domain

Artifacts (movements, partial volume effect, etc.)

...

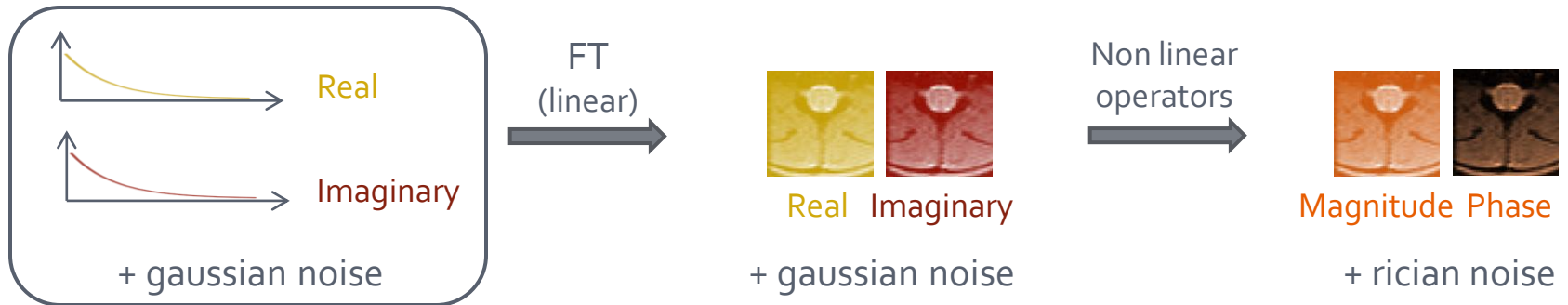
Noise correction and filter applied on magnitude images

Approximation of the attenuation signal by diffusion models

Main corrections during acquisition

Three methods were used to improve the SNR

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1. Averaging during acquisitions

Averaging n times $\rightarrow \sigma^2$ decreased by a factor \sqrt{n}

Three methods were used to improve the SNR

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2. Correction based on variance estimation from the background pixels

$$p_M(M) = \frac{M}{\sigma^2} e^{-\frac{(M^2+A^2)}{2\sigma^2}} I_0\left(\frac{A \cdot M}{\sigma^2}\right)$$

$$\text{if } A \approx 0 \quad p_M(M) = \frac{M}{\sigma^2} e^{-\frac{-M^2}{2\sigma^2}} \quad \hat{\sigma} = \sqrt{\frac{1}{2N} \sum_{i=1}^N X_i^2}$$

M : measured intensity
A : real intensity

if SNR > 3 Gaussian distribution of mean $\bar{M} = \sqrt{A^2 + \sigma^2}$

$$\tilde{A}_i = \sqrt{|M_i^2 - \hat{\sigma}^2|}$$

Three methods were used to improve the SNR



3. Non-Local Mean (NLM) Filter (Buades et Morel)

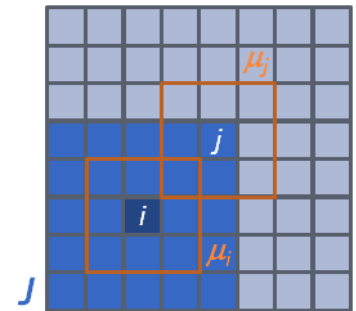
Smoothing filter that preserves borders and details

$$NL(\tilde{A}_i) = \sum_{j \in I} w(i, j) \tilde{A}_j$$

with $\sum_{j \in I} w(i, j) = 1$

$w(i, j)$: weighting function depending on the similarity between voxels i and j

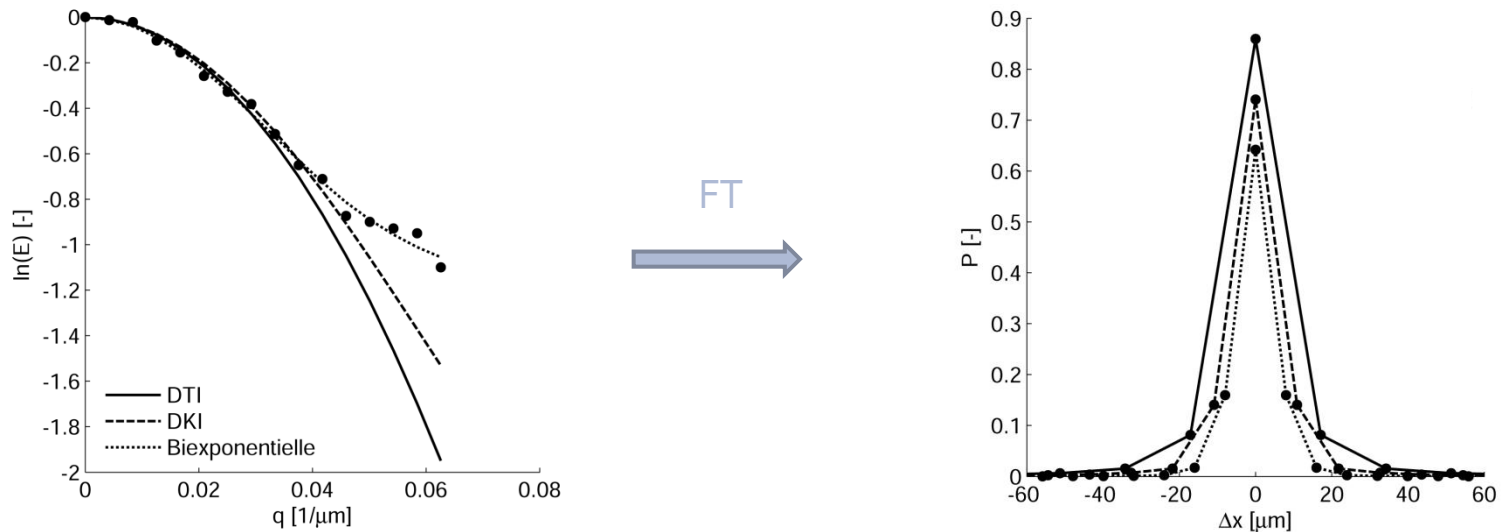
$$w(i, j) = \frac{1}{Z(i)} e^{-\|\tilde{A}_{\mu_i} - \tilde{A}_{\mu_j}\|_{2,a}^2 / h^2}$$



In vivo evaluation of the axonal degeneration
after spinal cord injury
using diffusion MRI and **DKI**

The DTI and the DKI are two diffusion models

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$$E(q) = \boxed{e^{-Aq^2D}} + Bq^4D^2K_1 + O(q^6)$$

Diffusion Tensor Imaging

Diffusion Kurtosis Imaging

DTI provides a first estimation of the parameters

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$$E(q) = \left[e^{-Aq^2D} + Bq^4D^2K \right] + O(q^6)$$

Diffusion Tensor Imaging

$$\ln(E(q)) = -Aq^2D$$

Simple linear regression
(least squares)

Diffusion Kurtosis Imaging

$$\ln(E(q)) = -Aq^2D + Bq^4D^2K$$

Non linear optimization
using trust-region-reflective algorithm
implemented in Matlab

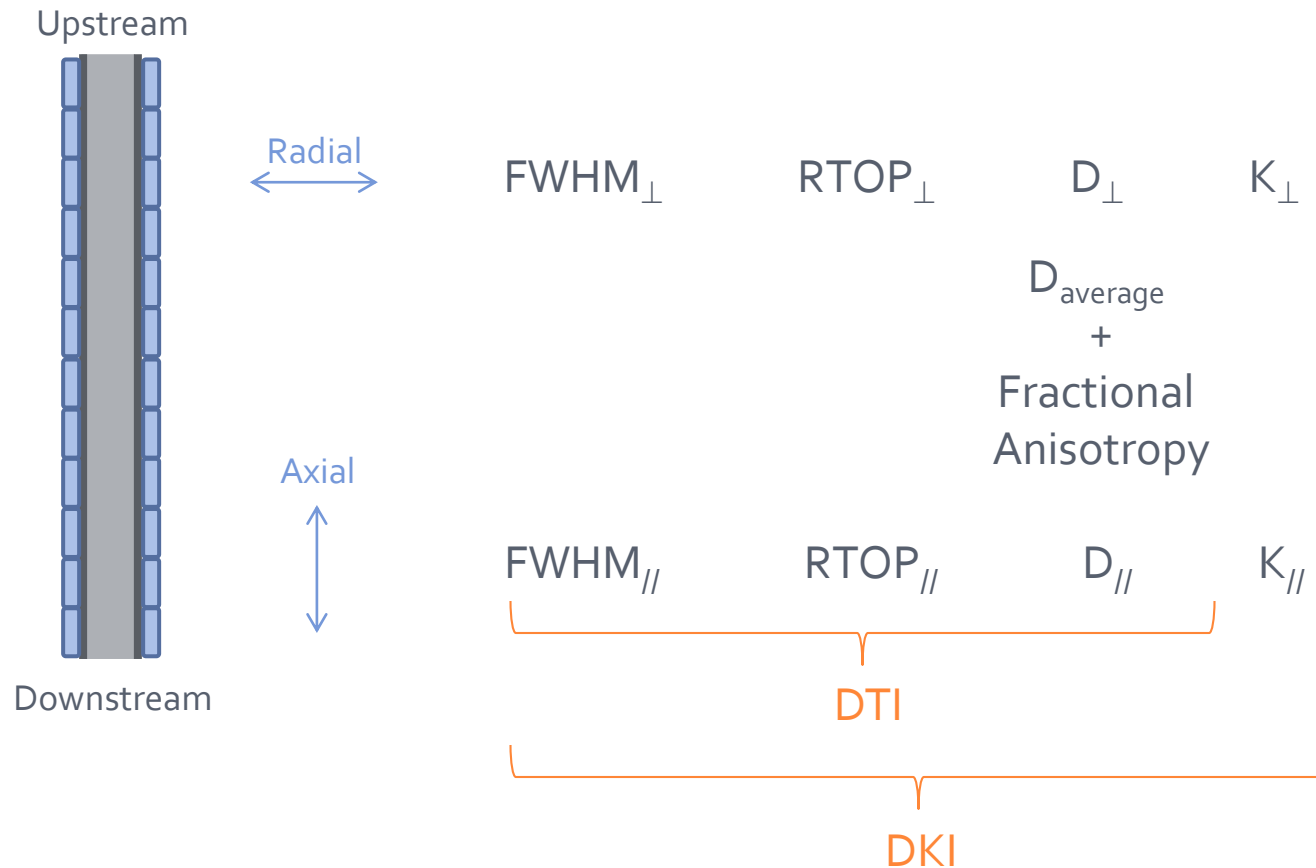
$$D, K > 0$$

$$D_0 = D_{DTI}$$

$$K_0 = 0$$

The final step is the extraction of parameters of the pdf

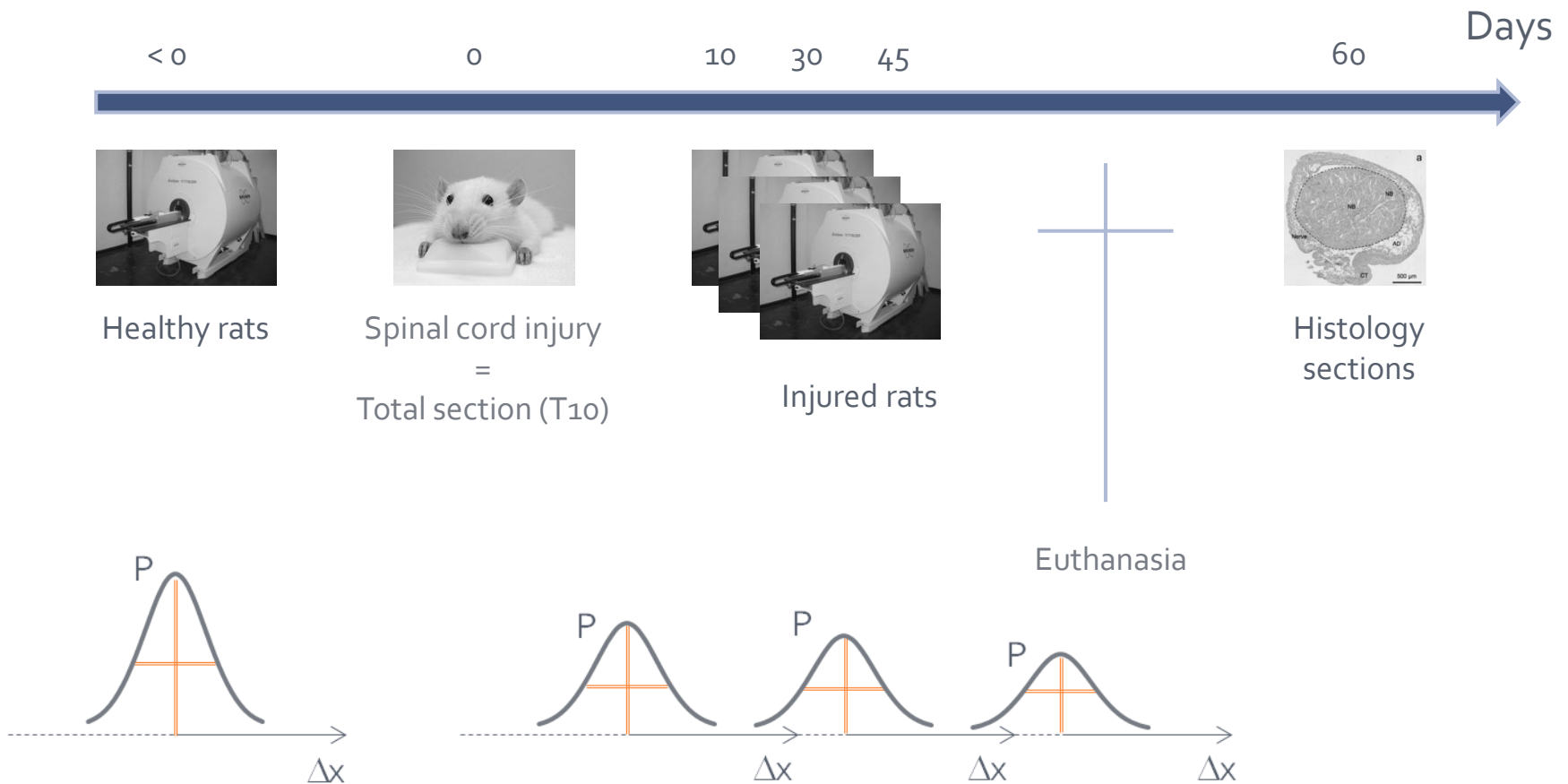
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In vivo evaluation of the axonal degeneration
after spinal cord injury
using diffusion MRI and DKI

The technique is adapted for longitudinal studies

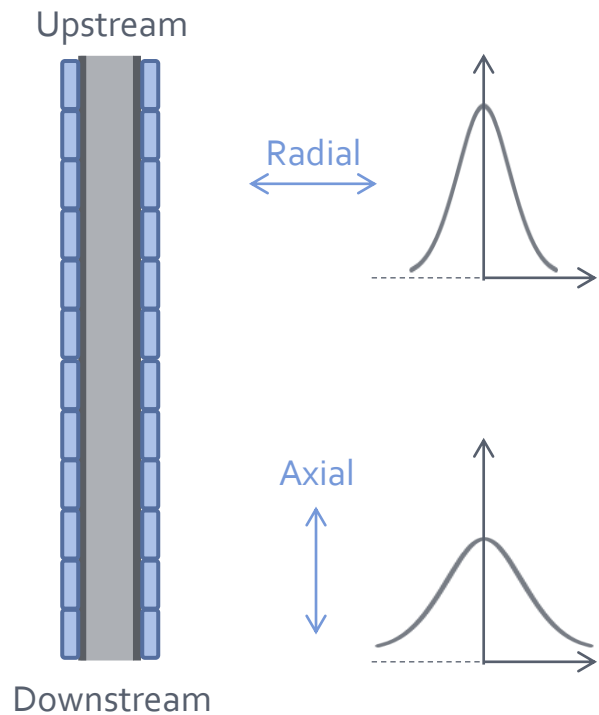
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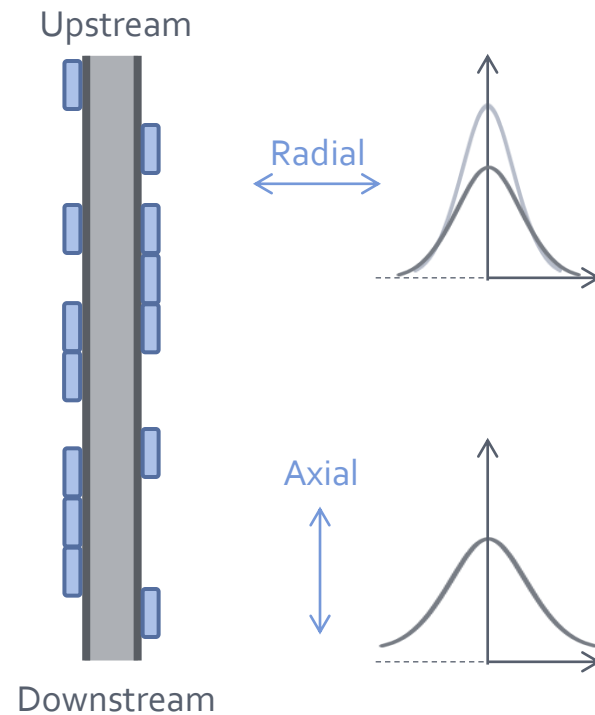
The evolution of the pdf shape gives information on the neuropathology

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Healthy rat



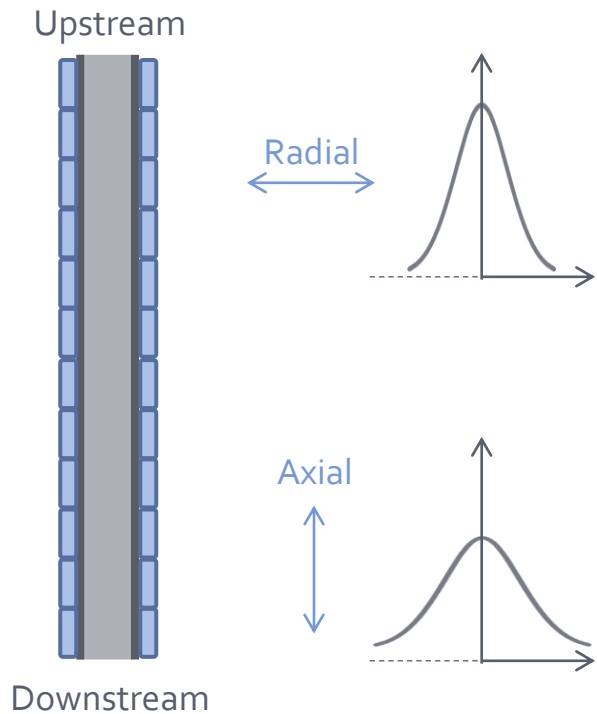
Demyelination



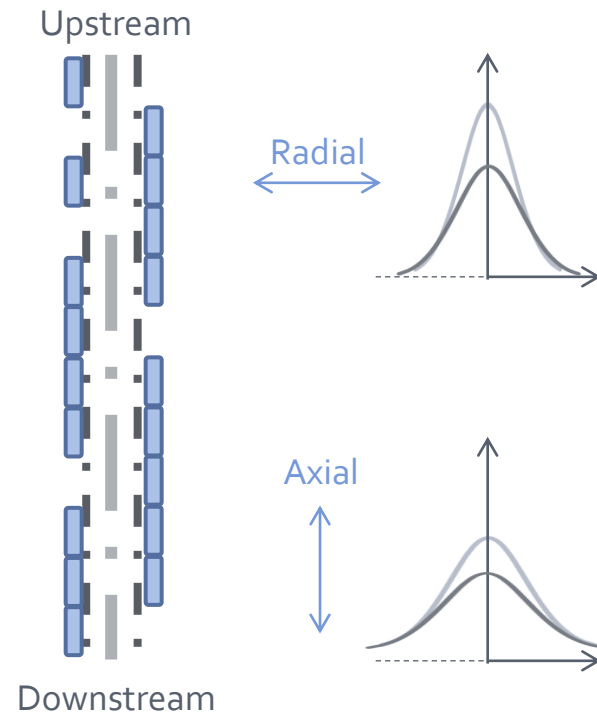
The evolution of the pdf shape gives information on the neuropathology

23

Healthy rat



Wallerian degeneration after section (distal part)



Further analysis of the results is based on diffusion maps

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- ... comparison between the four different acquisition times
- ... comparison between the upstream and the downstream parts of the lesion site
- ... comparison with histological sections
- ... estimation of good indicator(s) of the axonal degeneration

Falls can be tragic... so, be careful!

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Any questions ?